

paper

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1 **Effects of corrective insole on leg muscle activation and lower extremity**
2 **alignment for farmers with pronated foot**

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Abstract

10 *Background:* Previous research indicates the nature of certain work environments may cause healthy
11 workers to experience significant performance deterioration comparable to physical disability. Execution
12 of strenuous activities in conjunction with slippery and viscous muddy working terrain in rice cultivation
13 leads to a high prevalence of farmer musculoskeletal disorders and malalignments. Recommended
14 intervention strategies originally designed for congenitally disabled individuals may also be applicable to
15 farmers, including a simple corrective wedge to reduce foot eversion. The objective of the present study
16 was to investigate the effects of corrective wedges on lower extremity muscle activity and alignment when
17 subjects stood on flat rigid ground or muddy terrain, simulating typical work conditions encountered by
18 Thai rice farmers.

19 *Methods:* Nine healthy farmers with pronated feet were recruited to participate in the study and wedges
20 were custom fabricated for each participant based on physical therapy assessment and by using rapid
21 prototyping techniques. Participants were asked to stand barefoot or with wedges on the two surface types.

22 *Results:* Results showed that foot pronation and knee valgus improved (average of 5.5 – 16.1 degrees) when
23 participants were equipped with corrective wedges. The muscle activity of the peroneus longus and the
24 tibialis anterior increased for muddy terrain, as compared with the rigid surface. In general, the wedges
25 induced less tibialis anterior activity and greater peroneus longus activity compared to when participants
26 were standing barefoot. An elevation in evertor muscle activity may reflect stretching of the shortened
27 muscle as a result of the reduced degree of foot pronation.

28 *Conclusions:* The findings demonstrate the positive effects of corrective insole usage for farmers with
29 pronated feet, including improved lower extremity alignment and inverter muscle activity reduction for
30 both rigid and muddy terrains.

31

32 **Keywords:** Medial wedge insole; muscle activity; foot pronation; lower extremity alignment; working
33 surface condition

34

35 **1. Introduction**

36 The nature of certain work requirements and environments has been identified as cause of
37 healthy workers performance degradation comparable to physical disabilities [1, 2]. For example,
38 foot pronation, which can be defined as the motion of the foot articulations that allow the foot to
39 become more prone to the supporting surface, thereby increasing the ground contact surface area
40 of the foot [3]. Excessive foot pronation can result from a loss of muscle control due to neurological
41 dysfunction [4, 5]. Such muscle injury conditions may also occur in rice farmers due to
42 compensation for foot instability and control of body alignment while walking on slippery and
43 highly viscous mud in rice paddy fields [6, 7]. The extreme environment and strenuous work
44 requirements of certain rice cultivation processes causes farmers to develop a high prevalence of
45 musculoskeletal disorders (MSDs) and malalignments in various body parts [8; 9]. The prevalence
46 of MSDs among rice farmers in Thailand has been found to be between 10.3-73.3% [10]. In a
47 recent study which investigated indications and triggers of musculoskeletal and lower limb
48 disability conditions [11], foot pronation was identified as the predominant disorder among rice
49 farmers in Khon Kaen, Thailand, with a percentage of 36.1%. An analysis of the risk factors
50 showed that years of farming experience correlated strongly with the specific type of foot
51 malalignment.

52 Rice farming activities in Thailand mostly involve manual labor (National Statistical Office),
53 which includes frequent lifting of heavy loads and requires awkward postures and prolonged
54 standing [12]. In addition, the preference of farmers to perform their work with bare feet is
55 suspected to aggravate MSDs and lower limb malalignments, as viscous muddy paddy fields
56 increase force loading on joints and muscles of the lower extremities [13]. In addition, abnormal
57 foot structures can further raise the risk of lower limb injuries [14, 15], while abnormalities in foot
58 pronation might result in passive hypermobility and instability of specific joints in the foot [16].
59 Consequently, individuals suffering from pronated feet may feel unstable during weight bearing,
60 demonstrate poorer balance, and demonstrate a higher risk of injury due to slipping or falling [17].
61 In addition, there is evidence of a close relationship between variations in foot structure among
62 healthy individuals and the risk of lower limb injury, possibly due to changes in lower limb muscle
63 activity [18]. This research indicated individuals with pronated feet depend on additional muscular
64 support while walking or running [18] and induced fatigue can increase the risk of injury [19].

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65 However, despite knowledge and general awareness of the above hazards, successful intervention
66 designs for rice farmers are limited [20, 21].

67 Studies of intervention strategies for individuals with disabilities have suggested methods
68 could also be applied to support healthy individuals working in extreme environments or aid in
69 prevention of occupation-related injury [2]. Along these lines, our previous work revealed
70 similarities in pain perception, malalignment, and origin of structural impairment between patients
71 with a neurological disorder, specifically cerebral palsy (CP) with spastic diplegia, and rice farmers
72 [7]. Patients diagnosed with CP showed extensive knee valgus and foot pronation, matching well
73 with clinical symptoms observed among rice farmers. A subsequent study reviewed and
74 recommended several ergonomic interventions, originally designed for CP patients, to be
75 applicable to rice farmers [22]. The study revealed most existing and proposed interventions for
76 farmers are based on educational programs and tool redesigns. There has also been no attempt to
77 adapt readily available interventions for congenitally disabled populations, including patients with
78 CP, for the healthy farmer workforce. 2
79 Based on previous study [22], it concluded that orthotic
80 devices could have great value for treatment of foot pronation, which is in-line with other clinical
81 and rehabilitation medicine studies proposing applications of molded foot orthoses [23],
82 removable external orthotic devices [24, 25], and inserts or specially designed insoles [26, 27].
83 However, molded orthotics are expensive and require many manufacturing steps in production of
84 specific structural elements. Moreover, molded orthotics are difficult to fit into existing footwear
85 due to bulkiness of the material [28]. Removable external orthotic devices (e.g., ankle foot
86 orthoses) may restrict movement due to rigid designs; whereas, orthotics with adaptive control
87 systems are expensive and require an external power source [24, 25]. A simple wedge has been
88 proposed as an alternative treatment device and is often selected by medical practitioners to
89 provide patients with direct therapy. Such corrective wedges can be used in footwear where space
90 is restricted and require significantly less manufacturing time (up to 3 times less) and cost up to
91 2.5 times less, as compared with molded orthotics [27]. Recent advances in custom orthotic
92 production make use of 3D-scanning technology to acquire an appropriate model of the patient's
93 feet, as well as rapid prototyping to accelerate the production process [29, 30]. This procedure
94 allows custom orthotics to be quickly designed and manufactured and, therefore, represents a
highly practical means of development of interventions for rice farmers.

95 The objective of the present study was to investigate the effects of simple corrective wedges
96 on farmer leg muscle activity and foot and knee alignments, induced by standing on different work
97 terrain surfaces, including normal flat rigid ground and a muddy surface. The types of terrain were
98 selected based on conditions typically encountered by workers during performance of rice
99 cultivation tasks. It was hypothesized that wedge insoles would help to correct deviations of foot
100 and knee alignments. Muddy terrain was expected to induce greater muscle activity related to foot
101 inversion and eversion (i.e., tibialis anterior (TA) and peroneus longus (PL), respectively). A
102 proposed medial wedge insole was expected to help reduce muscle activity for both terrain
103 conditions and demonstrate applicability of orthotic devices, primarily used by the disabled
104 population, to extend to the agricultural workforce.

105

106 **2. Materials and methods**

107 *2.1. Participants*

108 Experienced rice farmers (males and females aged between 20-59 years) were recruited from
109 Khon Kaen Province, Thailand. Participants were required to have at least 1 year of experience in
110 rice cultivation and to have no prior medical history affecting lower extremity alignment, such as
111 surgery and/or a fracture. Subsequently, rear foot and medial longitudinal arch angles of all
112 participants were measured, based on Jonson and Gross's method [31]. The participants were
113 included in the study upon diagnosis of foot pronation (i.e. a rear foot angle greater than 9 degrees
114 and a medial longitudinal arch angle less than 134 degrees). The subject sample allowed for
115 investigation of changes in lower extremity alignment and muscle activity. The experiment was
116 conducted with a sample size of 9 subjects, based on previous studies in which the sample size
117 ranged from 9-70 subjects [26, 27]. All participants gave a written informed consent. Study of
118 these participants was approved by the Khon Kaen University Ethics Committee for Human
119 Research.

120

121 *2.2. Corrective insole design and fabrication*

122 Corrective insoles were custom designed and manufactured for each participant. The size of
123 the insoles was determined by the participants' shoe size, which was either 10", 10.5", or 11" in
124 the current study (Fig. 1). The fabrication process of corrective insole started from the reverse
125 engineering of the foot anatomy and according to the three steps, including (1) 3D anatomy

126 acquisition, (2) 3D CAD modeling of the corrective insole, and (3) 3D printing process of the
127 corrective insole.² On the data acquisition step, a scanning process was conducted using a 3D
128 scanner and a clinical examination conducted by physical therapists. A Sense 3D scanner (3D
129 Systems, Inc., Rock Hill, USA) was used for acquisition of a 3D image of each participant's feet
130 while the subject was seated with legs held out horizontally, supported on a stable chair of the
131 same height. On the 3D CAD modeling step, the 3D image of the foot was used to create a 3D
132 computer-based model of the insole and the custom filling of the arch using the SolidWorks
133 software package (Dassault Systèmes SolidWorks Corporation, Waltham, USA). Based on clinical
134 examination and measurement of foot malalignment (described in measurement of lower extremity
135 alignment section), the specific height and angle of the medial forefoot wedge, medial rear foot
136 wedge and heel lift (required to correct the individual foot alignment) were identified and
137 incorporated in the model. Specifically, a 1/8-inch (0.318 cm) heel lift was prescribed if
138 participants exhibited less than neutral dorsiflexion at the ankle. A medial forefoot wedge, with
139 the angular magnitude of measured forefoot varus, was included if the participant exhibited
140 forefoot varus more than or equal to 5 degrees. If the rearfoot angle of the participant was more
141 than 9 degrees, a medial rearfoot wedge was included, with the angular magnitude that corrected
142 the rearfoot angle to be less than 9 degrees but not exceed a 1/8-inch (0.318 cm) height of wedge.
143 Once the design was completed, the wedge insole was manufactured by printing polylactic acid
144 (PLA) filaments on a FlashForge 3D Printer Creator Pro (Zhejiang Flashforge3D technology
145 Co.,LTD, Jinhua, China).

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(A)

(B)

(C)

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Fig. 1. Examples of medial wedge insole design of sizes: (A) 10" (B) 10.5"; and (C) 11".

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152 2.3. Measurement of lower extremity alignment

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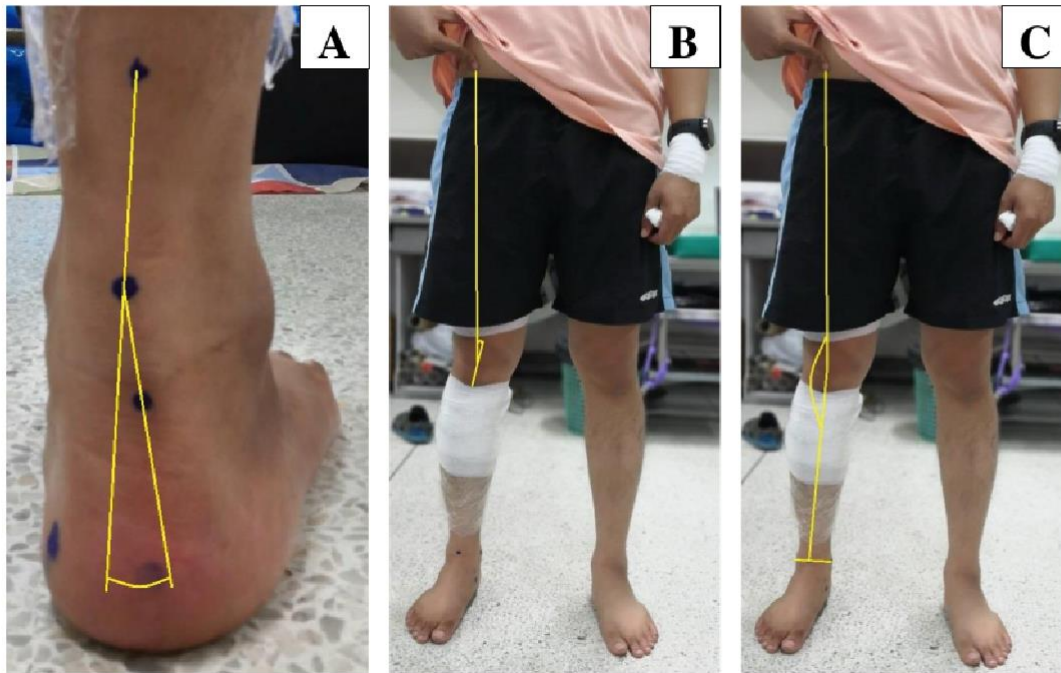
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As foot pronation and knee valgus are linked deformities, the alignments of rear foot angle, medial longitudinal arch angle, quadriceps (Q) angle, and tibiofemoral angle were measured in this study. The measurements were conducted in a standardized standing position and were based on the methods described in ([11], Fig. 2). All measurements were repeated 3 times by a single physical therapist. Participants' feet were classified as showing normal alignment when the rear foot angle ranged between 3 - 9 degrees and the medial longitudinal arch angle ranged between 134 - 150 degrees [31]. A genu valgus (knock-knee) was identified when the Q-angle was greater than 18 degrees or the tibiofemoral angle was less than 173 degrees. For normal knee alignment, the Q-angle of males and females is approximately 10–13 degrees and 15–18 degrees, respectively, and the tibiofemoral angle is approximately 173 -180 degrees [32, 33].

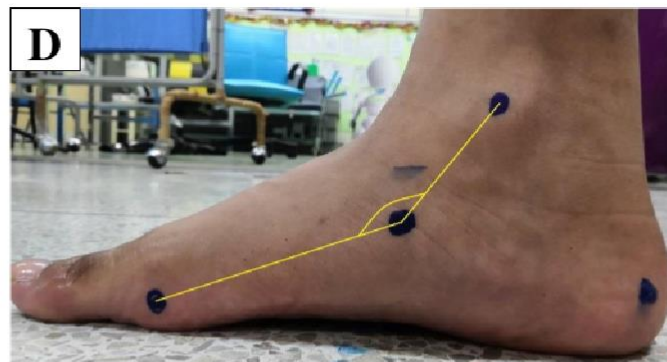
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171 Fig. 2. Lower extremity alignment measurement methods for: (A) rear foot angle; (B) quadriceps
172 angle; (C) tibiofemoral angle and; (D) medial longitudinal arch angle.

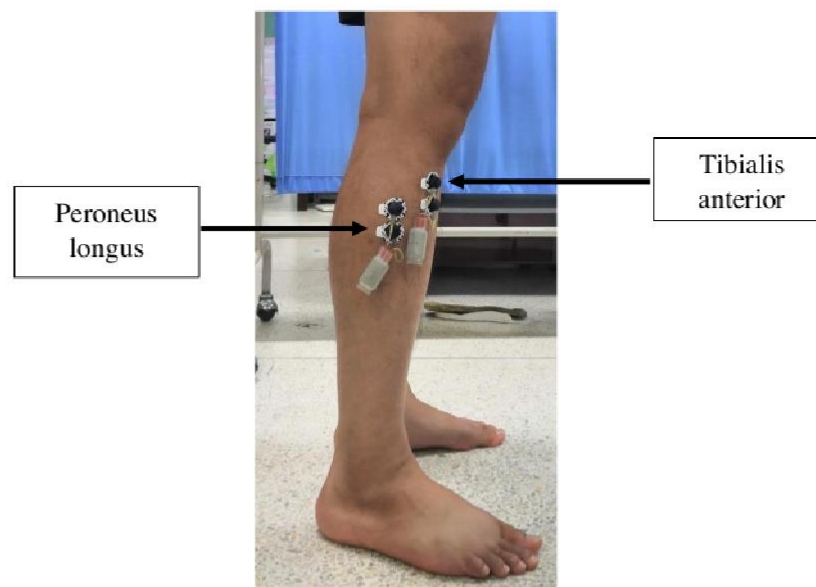
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174 2.4. Measurement of lower extremity muscle activity

175 The foot invertor and evertor muscles, TA and PL, respectively, were connected to a wireless
176 electromyograph (EMG; Wave Plus, Cometa, Milan, Italy), after which the EMG Easy Report

177 software (MerloBioEngineering, Parma, Italy) was used to measure and analyze muscle activity.
178 To reduce impedance, the skin underlying the electrodes was shaved, scraped with sand paper, and
179 cleaned with alcohol. Two pairs of surface EMG electrodes were placed 2 cm apart over
180 anatomical locations of TA and PL muscles, based on the guidelines from previous research [34].
181 Specifically, the electrodes were placed 3 cm below the fibular head to measure PL muscle activity,
182 and 1 cm lateral to the tibia edge and 8 cm below the tibial tuberosity to measure TA muscle
183 activity (Fig. 3). Muscle activity of the TA and the PL was collected simultaneously from the
184 participants' right leg at a sampling rate of 2000 Hz. EMG data were filtered using 20 – 500 Hz
185 bandpass and 50 Hz notch filters. The root mean square (RMS) values were obtained and
186 normalized as a percentage of the maximal voluntary isometric contraction (%MVIC). The MVIC
187 value of the PL and TA were measured in the neutral ankle joint position, based on guidelines
188 from a previous study [35].

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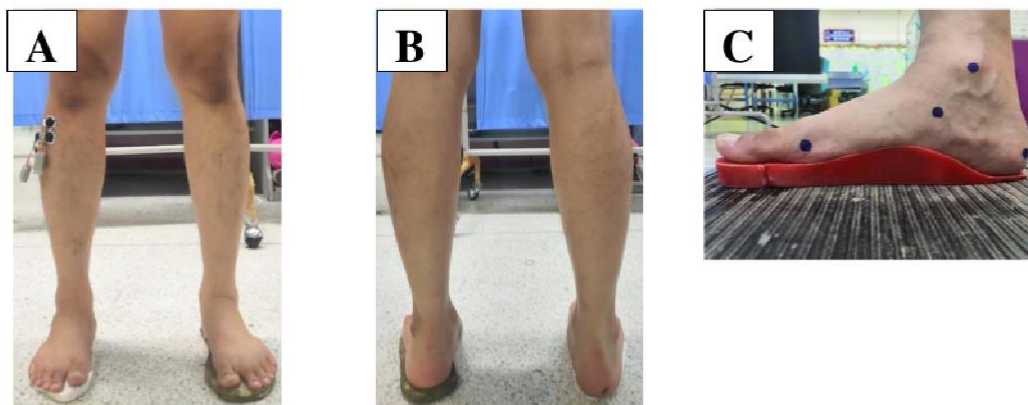
191 Fig. 3. Illustration of EMG electrode placements of peroneus longus (PL) and tibialis anterior
192 (TA).

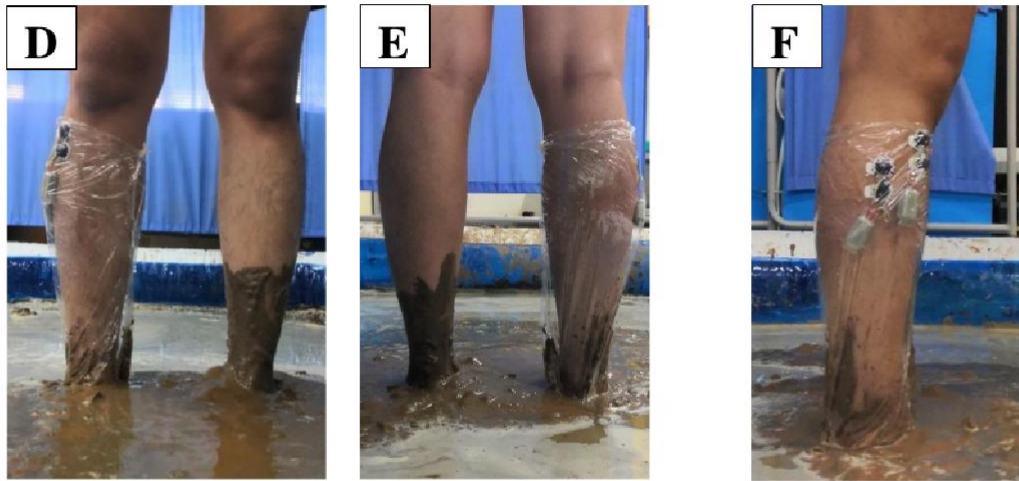
193 2.5. Experimental procedure

194 The study consisted of two footwear conditions, (1) barefoot (BF) and (2) with corrective
195 insole (CI); and two work terrain surfaces, (1) flat rigid and (2) muddy surface. For the latter

196 condition, we used a mud-filled container with a flat bottom surface. The order of participant
197 exposure to the experimental conditions was randomized. Before starting the experiment,
198 participants were given a 5-minute rest. Subsequently, they were instructed to assume a standing
199 position with a stance width of shoulder-width apart, maintain a stable posture, and look straight
200 ahead for 1 minute while lower extremity alignments were measured and EMG data were recorded.
201 Due to limited visibility, the foot alignments, including rear foot angle and medial longitudinal
202 arch angle, could not be measured when participants were standing in the mud. Fig. 4 illustrates a
203 participant equipped with corrective insoles standing on the two work terrain conditions. All
204 participants were provided a 5-minute break between each experiment condition to relieve any
205 potential muscle fatigue, based on a recommendation from prior research [36]. To prevent potential
206 injury through falling or slipping, the corrective insoles were secured by plastic wraps to the
207 participants' feet while standing on muddy terrain.

208





209 Fig. 4. Illustration of standing posture with corrective insoles: (A-C) front, back and medial
 210 view (to demonstrate a thickness of wedge) on flat rigid terrain and; (D-F) front, back and
 211 lateral view (due to a difficulty to obtain the medial side of foot) on muddy terrain.

212

213 3. Results

214 3.1. Demographic data of participants

215 Relevant participant characteristics are displayed in Table 1. The age of the participants ranged
 216 from 40 - 62 years and their experience in rice farming ranged from 15 - 49 years. Most participants
 217 wore 10.5" footwear. All participants exhibited excessive foot pronation identified by abnormal
 218 rear foot and medial longitudinal arch angles, as well as excessive knee valgus identified by
 219 abnormal Q or tibiofemoral angles.

220

221

Table 1. Participants characteristics

Characteristics	n (%)	Mean (SD)
Gender		
Male	4 (44.44)	
Female	5 (55.56)	
Age (years)		51.89 (6.86)
Height (cm)		161.78 (6.10)
Weight (kg)		59.80 (11.70)

Experience (years)		36.11 (9.71)
Size of footwear		
Size 10	1 (11.11)	
Size 10.5	6 (66.67)	
Size 11	2 (22.22)	
Rearfoot angle (deg)		10.70 (1.57)
Normal	0 (0)	
Abnormal	9 (100)	
Medial longitudinal arch angle (deg)		128.65 (2.38)
Normal	0 (0)	
Abnormal	9 (100)	
Q-angle (deg)		21.49 (1.88)
Normal	0 (0)	
Abnormal	9 (100)	
Tibiofemoral angle (deg)		170.82 (2.31)
Normal	0 (0)	
Abnormal	9 (100)	

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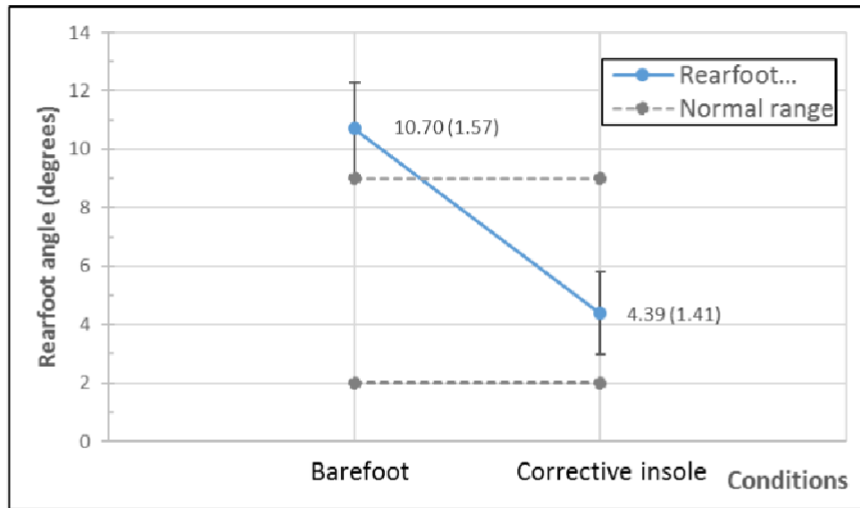
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224 *3.2. Lower extremity alignment*

225 The angle measurements for lower extremity alignment of participants are presented in Figs.

226 5-8.

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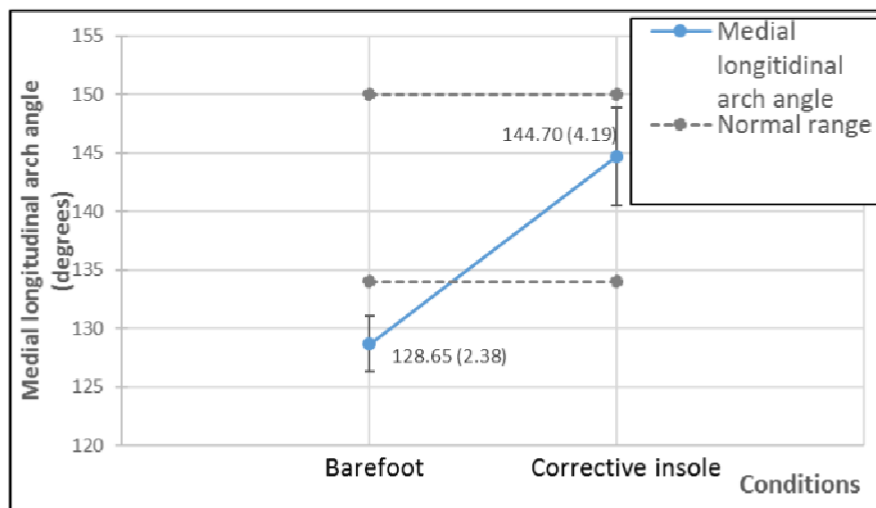


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Fig. 5. Results of rearfoot angle alignment for rigid work terrain condition

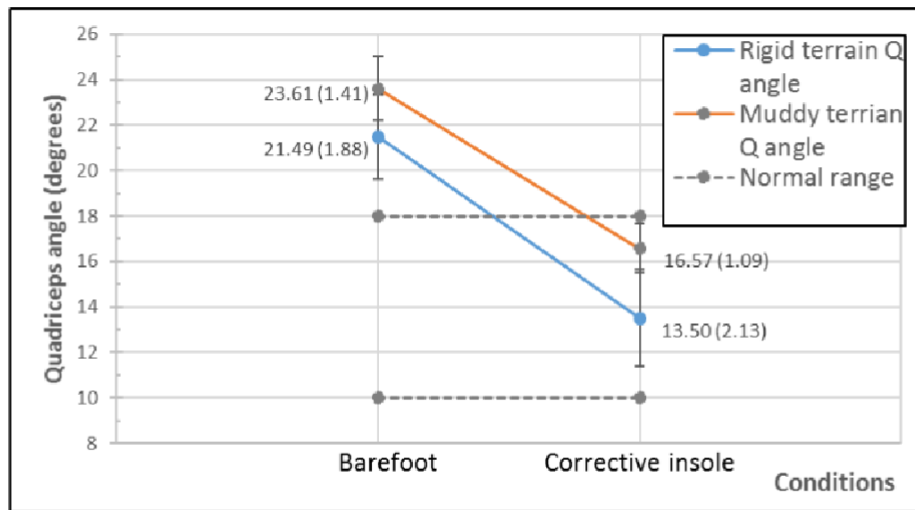


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Fig. 6. Results of medial longitudinal arch angle alignment for rigid work terrain condition

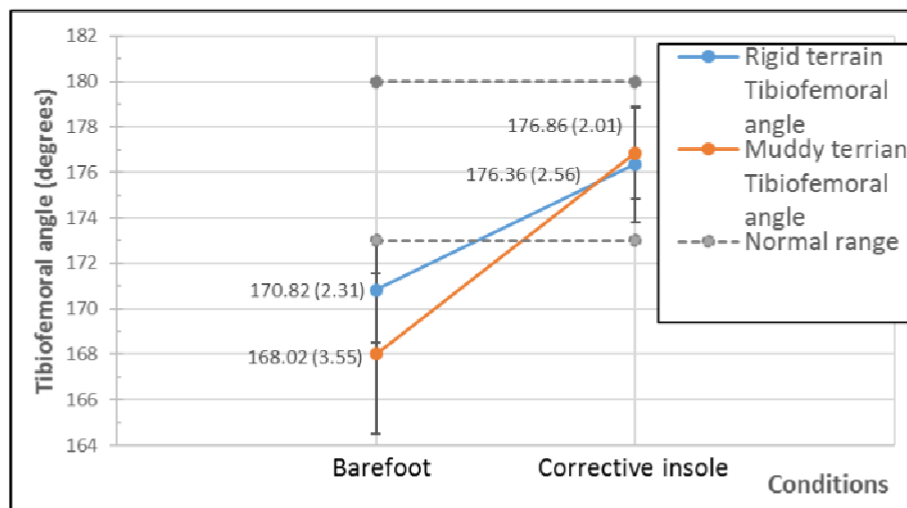


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Fig. 7. Results of Q-angle alignment for various experimental terrain conditions



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Fig. 8. Results of tibiofemoral angle alignment for various experimental terrain conditions

240 3.3. Lower extremity muscle activity

241 The comparison of PL and TA muscle activity between BF and CI conditions during standing
 242 on flat rigid and muddy terrains is presented in Table 2.

243

244

245 Table 2. Mean (SD) of muscle activity involved during flat and muddy terrain standing
 246 position

Muscle activity (%MVIC) (mean (SD))	Conditions			
	Barefoot (BF)		Corrective insole (CI)	
	Rigid terrain	Muddy terrain	Rigid terrain	Muddy terrain
Tibialis anterior (TA)	0.80 (0.22)	1.32 (0.20)	0.69 (0.19)	1.04 (0.21)
Peroneus longus (PL)	1.01 (0.19)	1.69 (0.16)	2.43 (0.23)	2.59 (0.41)

247

248 **4. Discussion**

249 *4.1. Lower extremity alignment*

250 Results show that the muddy terrain induced an increase in Q-angle for all participants (average
 251 increase of deviation of 0.5 – 2.8 degrees), likely due to the slippery surface posing a greater
 252 demand to control leg alignment. This situation may lead to postural instability and fatigue,
 253 therefore increasing foot and knee pain [37]. In agreement with expectation, participants showed
 254 abnormal alignments of the lower extremities when standing barefoot (BF condition) on both flat
 255 rigid ground and in muddy terrain. When the participants were equipped with corrective medial
 256 wedge insoles (CI condition), all lower extremity alignments showed less deviation (average
 257 improvement of 5.5 – 16.1 degrees) and could be identified as normal.

258 A number of corrective insoles have been investigated in previous studies. For example, studies
 259 that observed an average reduction in angles of foot eversion of 2.1-5.5 degrees during movement
 260 [27, 28] , whereas in the present study, rearfoot angles were reduced by approximately 6.3 degrees.
 261 This greater reduction might be due to differences in participant characteristics (older vs. younger
 262 participants), body movement (standing vs. walking or running), and material for fabrication of
 263 the insoles (rigid PLA vs. flexible Ethylene Vinyl Acetate (EVA)) compared to previous studies.
 264 Participant movement and use of less stiff material for insoles might result in less reduction in the
 265 degree of foot eversion. Moreover, the plastic wrap used to secure the insoles in the present study
 266 might have provided additional support over and above the corrective insoles, and may have
 267 altered the results of lower extremity alignment.

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271 4.2. Lower extremity muscle activity

272 ² Results demonstrate that the muddy terrain resulted in greater activity of both invertor and
273 evertor muscles, which indicates an attempt to increase muscular force to compensate for
274 instability when standing in mud. For both terrain conditions, CIs induced lower TA muscle
275 activity in agreement with our hypothesis. As an increase in contraction of the TA muscle
276 contributes to deceleration of subtalar joint pronation moment [38], a decrease of TA muscle
277 activity could be attributed to a successful CI intervention reducing foot pronation for both rigid
278 and muddy terrain. Although a reduction of TA activity was clearly observed, differences were
279 still relatively small, presumably due to the smooth low-friction surface of the PLA insole. Indeed,
280 a previous study showed insoles with textured surface significantly decreased TA activity during
281 stance phase [39]. Future development of wedge insoles should investigate the effects of textured
282 surfaces, non-slip pads, or alternative materials on TA activity reduction.

283 Contrary to expectation, participants exhibited greater PL muscle activity when they stood on
284 a CI as compared with the BF condition. Previous research indicates that a pronated foot structure
285 is correlated with greater EMG amplitude for invertor muscles (e.g. TA) and less EMG amplitude
286 for evertor muscles (e.g. PL), when compared to supinated or normal foot structures [18, 40]. The
287 lower amplitude of the PL may be attributed to slight shortening of the muscle in the pronated
288 position [16], limiting the range of motion and functional movement. The increase in mean activity
289 of the PL muscle might reflect stretching, due to a lower degree of foot pronation when supported
290 by a medial wedge insole. A previous study also reported an increase of PL maximum amplitude
291 in asymptomatic participants with a medial wedge assisting lateral ankle stability, as compared to
292 walking with common footwear [41].

293

294 **5. Conclusions**

295 The present study investigated the effects of simple corrective insoles on foot muscle activity
296 as well as foot and knee alignments of farmers with pronated feet when they stood on rigid flat
297 and muddy surfaces. A corrective medial wedge was selected for investigation due to its
298 practicality for use by farmers in a rice paddy field, low production cost and time, and effectiveness
299 in treatment of foot pronation. Corrective wedges were custom fabricated for each participant
300 based on physical therapy assessment, 3D optical scanning and rapid prototyping techniques. The

301 total time to complete the fabrication process was approximately 6 hours, which can be considered
302 practical for custom-made products.

303 Results of the study showed that the muddy terrain induced greater deviation in knee
304 alignments and produced increased activation of extrinsic foot muscles, which may result in
305 fatigue for farmers. Therefore, working in muddy terrain is anticipated to increase lower extremity
306 muscle pain and risk of injury. **The proposed corrective insoles were found to help reduce TA
307 muscle activity, which is necessary for decreasing foot pronation, in both muddy and rigid terrain
308 conditions. The medial wedge insole also helped reduce foot pronation malalignment and served
309 to stretch shortened PL muscles.**

310 These findings demonstrate the positive effects of corrective insole usage on foot muscles and
311 alignments for both rigid and muddy terrains. However, the relatively small number of rice farmers
312 exhibiting foot pronation and participating in the study represents a limitation of the current work.
313 Follow-up research is expected to include a greater number of participants, both with and without
314 foot pronation, with the objective of identifying broadly effective methods for correcting and
315 preventing common risks of lower extremity injury. Furthermore, the actual use of the corrective
316 insoles for work will require some method to fix the insoles against the worker's feet (e.g., shoes,
317 sandals, etc.). Such fixation methods will likely interact with the insoles to exert influence that will
318 be different than just standing on the insoles as in this study. Future research will also include the
319 development of assistive intervention techniques in the form of footwear for rice farmers,
320 including custom insoles, to be worn while working under various work terrain conditions.

321

322 **Brief summary**

323 What is already known

- 324 • The nature of work environment may cause healthy workers having performance
325 worsening comparable to those of disabled people.
- 326 • The prevalence of MSDs among rice farmers in Thailand has been found very high.
- 327 • There are similarities in pain perception, malalignment, and origin of structural impairment
328 between patients with cerebral palsy (CP) and rice farmers.

329

330

331

332 What this study adds

- 333 • The foot pronation and knee valgus improved when participants were equipped with
334 corrective wedges.
- 335 • The wedges induced less tibialis anterior activity and greater peroneus longus activity
336 compared to when participants were standing barefoot.
- 337 • The corrective insole usage demonstrated a positive effect to improve alignment and reduce
338 inverter muscle force.

339

340 **Acknowledgements**

341 We would like to acknowledge the participants of this study for their time.

342

343 **Conflict of interests**

344 The authors declare that they have no conflict of interests.

345

346 **References**

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paper

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